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1	Acute Cardiac Functional and Mechanical Responses to Isometric Exercise in Pre-
2	Hypertensive Males.
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- 26 Abstract
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28 Isometric exercise (IE) training has been shown to reduce resting arterial blood pressure 29 (ABP) in hypertensive, pre-hypertensive and normotensive populations. However, the acute 30 haemodynamic response of the heart to such exercise remains unclear. We therefore 31 performed a comprehensive assessment of cardiac structure, function and mechanics at rest 32 and immediately post a single IE session in 26-male (age 44.8 ± 8.4 years) pre-hypertensive 33 participants. Conventional echocardiography recorded standard and tissue Doppler measures 34 of left ventricular (LV) structure and function. Speckle tracking echocardiography was used 35 to measure LV global longitudinal, circumferential and radial strain and strain rate. From this 36 data, apical and basal rotation and rotational velocities, LV twist, systolic twist velocity, 37 untwist velocity and torsion were determined. IE led to a significant post exercise reduction 38 in systolic (132.6±5.6 vs. 109.4±19.6mmHg, p<0.001) and diastolic (77.6±9.4 vs. 39 58.8 ± 17.2 mmHg, p<0.001) blood pressure, with no significant change in heart rate (62±9.4 40 vs. $63\pm7.5b\cdot \text{min}^{-1}$, p=0.63). There were significant reductions in LV end systolic diameter 41 (3.4±0.2 vs. 3.09±0.3cm, p=0.002), LV posterior wall thickness (0.99±0.1 vs. 0.9±0.1cm, 42 p=0.013), relative wall thickness (0.4±0.06 vs. 0.36±0.05, p=0.027) estimated filling pressure 43 (E/E' ratio 6.08±1.87 vs. 5.01±0.82, p=0.006) and proportion of participants with LV 44 concentric remodelling (30.8% vs. 7.8%, p=0.035), and significant increases in LV ejection 45 fraction (60.8±3 vs. 68.3±4%, p<0.001), fractional shortening (31.6±4.5 vs. 39.9±5%, 46 p<0.001), cardiac output (4.3±0.7 vs. 6.1±1L·min⁻¹, p<0.001), and stroke volume (74.6±11) 47 vs. 96.3±13.5ml, p<0.001). In this setting there were significant increases in global longitudinal strain (-17.8±2.4 vs. -20±1.8%, p=0.002) and strain rate (-0.88±0.1 vs. -48 49 1.03±0.1%, p<0.001), basal rotation (-5±3.5 vs. -7.22±3.3°, p=0.047), basal systolic rotational velocity (-51 \pm 21.9 vs. -79.3 \pm 41.3°·s⁻¹, p=0.01), basal diastolic rotational velocity (48.7 \pm 18.9 50

51	vs. $62.3\pm21.4^{\circ} \cdot s^{-1}$, p=0.042), LV twist (10.4±5.8 vs. 13.8±5°, p=0.049), systolic twist velocity
52	$(69.6\pm27.5 \text{ vs. } 98.8\pm35.8^{\circ} \cdot \text{s}^{-1}, \text{ p}=0.006)$, and untwist velocity $(-64.2\pm23 \text{ vs. } -92.8\pm38^{\circ} \cdot \text{s}^{-1}, \text{ p}=0.006)$
53	p=0.007). These results suggest IE improves LV function and mechanics acutely. This may in
54	turn be partly responsible for the observed reductions in ABP following IE training
55	programmes and may have important implications for clinical populations.
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- 76 Introduction
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78 Systemic arterial hypertension remains a significant global public health problem, which is 79 estimated to affect \approx 1-billion individuals worldwide (46) and is associated with considerable 80 morbidity and mortality. A sustained elevation in arterial blood pressure induces specific 81 compensatory cardiac maladaptations that are associated with poor prognosis, including left 82 ventricular hypertrophy, and systolic and diastolic dysfunction (1, 39), which through a 83 cascade of poorly defined events, progresses to clinically symptomatic heart failure (12). 84 85 International guidelines recommend non-pharmacological intervention, including regular 86 physical activity, salt restriction and weight loss for the primary and secondary prevention of 87 hypertension (14, 23). Evidence indicates an inverse, dose-dependent relationship between 88 levels of physical activity and cardiovascular disease, with reductions in blood pressure being 89 one proposed mechanism (14). The benefits of regular traditional aerobic training are well 90 documented, with improvements in maximal aerobic capacity, physiological cardiac 91 remodelling with coexistent improvements in systolic and diastolic function (2) and blood 92 pressure reductions (42). However, when compared to traditional aerobic and resistance 93 training (combined and in isolation), isometric exercise (IE) training has shown greater 94 reductions in arterial blood pressure (ABP) (6, 7).

A single bout of IE transiently decreases ABP in the minutes to hours following exertion
(24). The potential mechanisms responsible for this post exercise reduction are unclear, but
may include reduced vascular resistance and/or decreased cardiac sympathetic nervous
system activity (25). Indeed, these acute haemodynamic and cardiovascular responses have
been shown to be important mechanisms for the observed reductions in ABP following a

101	programme of IE training (8, 25). However, little is known regarding the effects of IE
102	training on cardiac performance both acutely and chronically. The acute cardiac responses to
103	a single IE session may, in part, provide a further mechanistic link to the observed reductions
104	in ABP seen following IE training. Therefore, we performed a comprehensive assessment of
105	cardiac function, including left ventricular (LV) strain, strain rate, rotation and twist at rest
106	and immediately post a single IE training session in a population with pre-hypertension (pre-
107	HTN).
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126 Materials and Methods

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- 128 Ethical approval and study population
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130 All procedures for this investigation conformed to the Declaration of Helsinki principles and 131 Canterbury Christ Church Universities Faculty of Social and Applied Sciences Research 132 Ethics Committee approved the study (Ref: 12/SAS/122). Signed, informed written consent 133 was obtained from all participants. We studied 26 physically inactive Caucasian males (age 134 44.8 ± 8.4 years; height 178.1 ± 5 cm; body mass 89.9 ± 1 kg; body surface area 2.1 ± 1 m²) 135 classified as pre-hypertensive (defined as a blood pressure of 120-139 mmHg systolic and/or 136 80-90 mmHg diastolic) with no history of cardiac or metabolic disease, non-smokers 137 currently taking no medication, and with a normal clinical cardiovascular examination and 138 12-lead electrocardiogram. We aimed to study a population with pre-HTN, who were 139 otherwise healthy for three main reasons; firstly, the homogenous population reduces the 140 impact of other co-morbidities on cardiac responses, secondly, pre-HTN precedes the 141 development of hypertension, and thirdly, cardiac mechanical responses in this group may 142 provide important mechanistic information for blood pressure reduction, which may prove 143 important for future IE training interventions in hypertensive populations.

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145 **Experimental procedures**

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Participants attended the laboratory on three separate occasions each separated by 48-hours
and were required to fast for 8-hours and abstain from caffeine and alcohol for 24-hours
before testing. All participants were required to maintain their normal circadian and dietary
patterns and attend the laboratory at the same time of day. The first session comprised of

initial resting blood pressure assessment to confirm pre-HTN. Each participant was seated for
15 minutes with the cuff at heart level. After this, three resting automated blood pressure
measurements were performed (Dinamap Pro 200 Critikon, GE Medical Systems, Freiburg,
Germany) (32) at five minute intervals and the avaerage recorded (23, 30).

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156 Prior research has demonstrated that when constant electromyography (EMG) is used to 157 determine exercise intensity, a steady state heart rate was achieved at 10, 15, 20, 25, and 30% 158 EMG (43). This physiological response established the potential for IE training prescription 159 via heart rate. Subsequent to this, research from our laboratory has demonstrated that 160 isometric wall squat intensity could be adjusted by manipulating knee joint angle, which 161 resulted in reliable heart rate responses (15). This method of isometric exercise prescription 162 elicited similar cardiovascular responses to other IE modes and has recently been shown to 163 significantly reduce resting blood pressure (45). As such, IE intensity was determined based 164 on participant heart rate and blood pressure responses to an incremental isometric exercise 165 test (43) using the wall squat as previously described (15). Participants were required to rest 166 their back against a fixed wall with their feet parallel, shoulder width apart, and their hands 167 by their side. Participants were instructed to lower their back down a solid wall, and make 168 small adjustments to their feet position until the required knee joint angle was reached whilst 169 maintaining a vertical lower limb and an erect trunk. Knee joint angle was measured using a 170 clinical goniometer (MIE Medical Research, Leeds, UK), secured to the participants lower 171 and upper leg using elasticated Velcro strapping. The test consisted of five consecutive 2-172 minute stages, beginning at a knee joint angle of 135° and guided to reduce the angle by 10° 173 every 2-minutes (125°, 115°, 105°, and 95°) (Figure 1). Each participants feet position was 174 measured from the back of the left heel to the wall and their back position was measured as 175 the distance from the ground to the lower back, which was defined as the lowest point of

176 contact that the participants back had with the wall. Participants were not permitted to stand 177 or rest between angles, and maintained the wall squat until volitional exhaustion or 178 completion of the 10-minute test. Verbal encouragement was given throughout, with 179 particular instructions to maintain normal breathing to avoid the Valsalva manoeuvre. Rating 180 of perceived exertion (Borg CR10 scale) was recorded at the end of each stage and/or test 181 termination, to obtain a subjective indicator of effort. Heart rate and blood pressure were 182 monitored continuously during the test using a plethysmographic device (Task Force[®]) 183 Monitor, CNSystems, Graz, Austria) to ensure participants remained within safe exercising 184 limits defined by American College of Sports Medicine.

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The mean heart rate for the last 30-seconds of each completed incremental stage was recorded. Prior research has demonstrated that knee joint angle produced an inverse curvilinear relationship with heart rate (15). As such, knee joint angle was plotted against mean heart rate for the last 30-seconds of each stage. The inverse curvilinear relationship produced was used to calculate each participants knee joint training angle that would elicit a target training heart rate of 95% peak heart rate as used in prior research (9, 44).

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193 On the second visit, each participant performed a familiarisation IE training session at their 194 prescribed training angle (mean $106 \pm 7^{\circ}$), which consisted of four 2-minute isometric wall 195 squats interspersed with 2-minutes recovery. On the third visit, each participant repeated the 196 single IE training session at their prescribed training angle and physiological data was 197 recorded pre and immediately post the IE session.

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201 Conventional echocardiographic image acquisition

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203 Transthoracic echocardiography was performed using a commercially available, portable 204 ultrasound system (Vivid-q, GE Healthcare, Milwaukee, Wisconsin) with a 1.5 – 3.6 MHz 205 phased array transducer (M4S-RS Matrix cardiac ultrasound probe), pre and immediately 206 post the single IE training session. The same sonographer acquired all images, with the 207 participant examined in the left lateral decubitus position. Cardiac structural and functional 208 measurements were recorded as recommended by current guidelines (21). Three consecutive 209 cardiac cycles were recorded and stored for offline analysis using commercial software on a 210 proprietary workstation (EchoPAC; V.113.0.x, GE Healthcare), with the results averaged. 211 Images were acquired in parasternal long-axis and short-axis (level of mitral valve and apex), 212 and apical 2-, 3-, 4-chamber views at baseline (following 15-minutes of supine rest) and 213 immediately post exercise. Interventricular septal and posterior wall thickness, fractional 214 shortening, and LV internal dimensions were recorded and relative wall thickness was 215 calculated as (2 x LV posterior wall thickness)/LV internal diameter. LV mass was calculated 216 according to (10) and indexed to body surface area. LV ejection fraction was determined by 217 the modified biplane Simpson's rule. The LV length was measured in the apical 4-chamber 218 view from the mitral valve plane to the most distal endocardium at the LV apex. Pulsed-wave 219 Doppler recordings were obtained to assess transmitral early (E) and late (A) diastolic filling 220 velocities from the apical 4-chamber view, with the sample volume placed at the tips of the 221 mitral valve. Isovolumic relaxation time was measured from the start of aortic valve closure 222 to mitral valve opening. Tissue Doppler imaging was acquired at the lateral and septal mitral 223 annulus to assess peak longitudinal (S'), peak early diastolic (E') and late diastolic (A') 224 velocities, with values averaged. LV filling pressure was estimated from the mitral E/E' ratios (28). Stroke volume was calculated by the product of LV outflow tract area and velocity time 225

integral from a pulsed wave Doppler signal placed in the LV outflow tract in an apical 5-

227 chamber view. Cardiac output was calculated as the product of stroke volume and heart rate.

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229 Cardiac mechanics: strain, rotation and twist

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231 Speckle tracking imaging was used to obtain global LV longitudinal strain and the time-232 derivative strain rate from the apical 2-, 3-, and 4-chamber views. LV radial and 233 circumferential strain and strain rate, and LV rotation and rotational velocity were obtained 234 from parasternal short axis views obtained from the LV base at the level of the mitral valve 235 (mitral valve leaflets on view) and the LV apex (circular LV cavity with no papillary muscle 236 visible), as described previously (22, 26, 37, 40) (Figure 2). For speckle tracking analysis, the 237 highest quality digital images were selected and the endocardium was traced. A full thickness 238 myocardial region of interest was selected. The observer readjusted the endocardial trace line 239 and/or region of interest width to ensure an acceptable tracking score.

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241 Since basal and apical rotation are not acquired from the same cardiac cycle and to enable 242 comparison between and within subjects, raw frame-by-frame rotation and rotation rate data 243 was normalised to the percentage duration of systole and diastole using cubic spline 244 interpolation (GraphPad Prism 6 Software, California, USA) (4, 5, 34). Subtraction of the 245 basal data from the apical data at each time point was undertaken to calculate LV twist and 246 untwist (4, 5, 34). LV torsion was defined as LV twist per unit length and was calculated by 247 dividing the total twist by LV diastolic length. Images were optimised for sector width and 248 scan depth in order to obtain high frame rates (>60 Hz) and kept constant for repeat 249 examinations. Intra and inter-observer variability was performed on 12 randomly selected participants and correlation coefficients using linear regression ranged from $r^2 0.92$ to $r^2 0.95$. 250

253	Measurements are presented as mean \pm standard deviation. All data were analysed using the
254	statistical package for social sciences (SPSS 22 release version for Windows; SPSS Inc.,
255	Chicago IL, USA). A paired samples T-test was used to compare baseline and post IE
256	measurements after confirmation of normal distribution. A chi-squared test was used to
257	compare categorical data. A p value <0.05 was regarded as statistically significant.
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276	Results
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278	General
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280	All 26-participants recruited completed the IE training session, which comprised of four 2-
281	minute isometric wall squats at each participants prescribed knee joint angle, interspersed
282	with 2-minutes recovery. Echocardiographic images suitable for complete analysis were
283	obtained on all subjects at rest and immediately post exercise.
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285	Haemodynamics
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287	There was a significant increase in cardiac output (4.3 ± 0.7 vs. 6.1 ± 1 L·min ⁻¹ , p<0.001),
288	predominantly mediated via a significant increase in stroke volume (74.6±11 vs. 96.3±13.5
289	ml, p<0.001) post exercise, since there was no significant change in heart rate (62±9.4 vs.
290	63 ± 7.5 b·min ⁻¹ , p=0.63). In addition, IE was associated with a significant reduction in
291	systolic (132.6±5.6 vs. 109.4±19.6 mmHg, p<0.001), diastolic (77.6±9.4 vs. 58.8±17.2
292	mmHg, p<0.001) and mean ABP (94.7±10.1 vs. 78.8±18 mmHg, p<0.001) in recovery.
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294	Cardiac function and structure: conventional and tissue Doppler parameters
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296	Baseline and post IE echocardiographic structural, functional and tissue Doppler parameters
297	are detailed in Table 1. There was a significant decrease in LV end systolic diameter (3.4 ± 0.2)
298	vs. 3.09±0.3 cm, p=0.002), LV posterior wall thickness (0.99±0.1 vs. 0.9±0.1 cm, p=0.013)
299	and relative wall thickness (0.4 ± 0.06 vs. 0.36 ± 0.05 , p=0.027) following the IE training
300	session with no change in LV end diastolic diameter, interventricular septal thickness or LV

- length. There was a significant increase in the proportion of participants with normal LV
 geometry following IE (69.2% vs. 92.2%, p=0.035).
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There was a significant increase in LV ejection fraction (60.8 ± 3 vs. 68.3 ± 4 %, p<0.001) and fractional shortening (31.6 ± 4.5 vs. 39.9 ± 5 %, p<0.001) following IE. There were no significant changes in global diastolic function; however, there were significant increases in LV tissue Doppler S' (0.09 ± 0.01 vs. 0.19 ± 0.04 , p<0.001) and E' (0.12 ± 0.02 vs. 0.15 ± 0.03 , p<0.001), with the latter resulting in a significant decrease in estimated filling pressure post IE (E/E' ratio 6.08 ± 1.87 vs. 5.01 ± 0.82 , p=0.006).

311 LV strain, rotation, torsion and untwisting

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313 Myocardial mechanics pre and post IE are displayed in Table 2. Global longitudinal strain (-17.8±2.4 vs. -20±1.8 %, p=0.002) and strain rate (-0.88±0.1 vs. -1.03±0.1 %·s⁻¹, p<0.001) 314 315 significantly increased post IE with no difference in global longitudinal diastolic strain rate 316 $(1.26\pm0.3 \text{ vs. } 1.37\pm0.3 \text{ }\% \cdot \text{s}^{-1}, \text{ p}=0.259)$. There was a significant increase in both basal and 317 apical circumferential strain (-28.9±5.4 vs. -34.8±6.3 %, p=0.003 and -25.3±4.1 vs. -32.9±7.6 %, p<0.001, respectively) and strain rate (-2.3 \pm 0.5 vs. -2.8 \pm 0.6 % ·s⁻¹, p=0.009 and -2.04 \pm 0.5 318 319 vs. $-2.57\pm0.7 \ \% \cdot s^{-1}$, p=0.012) and significant increase in apical radial strain (35.4±16.4 vs. 320 55 ± 17.8 %, p=0.001). There was a significant increase in basal rotation (-5±3.5 vs. -7.22±3.3 °, p=0.047), basal systolic rotational velocity (-51 \pm 21.9 vs. -79.3 \pm 41.3 °·s⁻¹, p=0.01) and 321 basal diastolic rotational velocity (48.7 \pm 18.9 vs. 62.3 \pm 21.4 °·s⁻¹, p=0.042); however, there 322 323 was no significant change in apical rotation, apical systolic rotational velocity and apical 324 diastolic rotational velocity. The increase in basal mechanics translated into a significant 325 increase in LV twist (10.4±5.8 vs. 13.8±5°, p=0.049), systolic twist velocity (69.6±27.5 vs.

326	98.8±35.8 °·s ⁻¹ , p=0.006), untwist velocity (-64.2±23 vs92.8±38 °·s ⁻¹ , p=0.007) and LV
327	length corrected torsion (1.46±0.86 vs. 2.07±0.88 °· cm ⁻¹ , p=0.032). Figure 3 displays the
328	composite twist, basal and apical rotation and rotational velocity curves with annotations
329	indicating key findings.
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351 **Discussion**

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353 To our knowledge, this study is the first to investigate the acute effects of isometric wall 354 squat exercise on cardiac structure, function and LV mechanics in men with pre-HTN. A 355 single IE training session was associated with a significantly reduced LV end systolic internal 356 diameter, LV posterior wall thickness, relative wall thickness and proportion of patients 357 characterised with concentric LV remodelling. These favourable LV remodelling responses 358 to acute IE are similar to those reported in patients with hypertension following a programme 359 of aerobic exercise training or prescribed diuretics (33). A single IE training session was 360 associated with improved global longitudinal, circumferential strain and strain rate and apical 361 radial strain as well as increased LV twist and untwist. These favourable responses in cardiac 362 mechanics have been demonstrated in healthy volunteers during aerobic exercise (27). Our 363 results suggest IE acutely improves LV remodelling, LV systolic and diastolic function and 364 LV mechanics. These positive adaptive changes may in turn contribute to the observed 365 reductions in ABP following IE training programmes (19) and have important implications 366 for clinical populations.

367

368 The mechanisms responsible for this acute response may in part be due to the significant 369 increase in cardiac systolic function and significant decrease in estimated LV filling pressure 370 and LV after-load. Indeed, Rinder et al. (2004) demonstrated a significant correlation 371 between reductions in systolic blood pressure and reduced relative wall thickness and 372 reported an increase in stroke volume, cardiac output and LV ejection fraction in their 373 exercise training group. Other lifestyle interventions, such as low sodium diets have 374 demonstrated significantly improved LV diastolic function with significantly reduced ABP in hypertensive heart failure patients (17, 18). Although not statistically significant, reductions 375

in LV mass index, relative wall thickness and increased LV ejection fraction, stroke volume,and cardiac output were also reported (18).

378

379 LV peak strains and strain rate have been proposed as indicators of regional myocardial 380 function (16). Our study demonstrated that global longitudinal and radial systolic function 381 improved post IE. This may in part be explained by a maintained pre-load, as suggested by 382 LV end diastolic dimensions, and increased contractility (decreased LV end systolic 383 dimension), mediating an increase in fractional shortening, LV ejection fraction and stroke 384 volume. The underlying mechanism may include an increase in excitation-contraction 385 coupling via improved cardiac calcium signalling as a result of sympathetic nervous system 386 activity and/or nitric oxide bioavailability. Nitric oxide has been reported to exert significant 387 effects on cardiac function, in particular LV relaxation and may modulate fundamental events 388 of myocardial excitation-contraction coupling (29). In addition, a recent animal study 389 demonstrated that dietary nitrate, which is known to reduce blood pressure, improves 390 cardiomyocyte calcium signalling and LV contractile function (31). 391 392 An acute IE training session induced a significant increase in LV twist and untwist, primarily 393 mediated by significant increases in basal rotation, basal systolic rotational velocity and basal 394 diastolic rotational velocity. Similar responses have been described following acute sub-395 maximal and maximal aerobic exercise (13). Amongst patients with treated hypertension, 396 reduced and delayed untwisting is reported with worsening LV remodelling, which may 397 contribute to LV relaxation abnormalities (35). Enhanced LV twist or torsional deformation 398 augments potential energy during the ejection phase and the recoil of this systolic 399 deformation and release of elastic energy (bi-directional spring) may contribute to pressure 400 decay, enhancing LV suction and associated diastolic filling (11, 20). Studies in human

volunteers reported that invasive measures of LV pressure and indexes of LV untwist are
related to parameters of early diastolic filling (5). These authors reported that reductions in
the rate and magnitude of untwisting were associated with worsening early diastolic suction
and supported the concept that untwisting is important in generating LV suction and
improving early diastolic filling (5). In our study there were no significant differences in
conventional measures of diastolic function.

407

408 The LV mechanical responses may in part be explained by mechanisms that also result in 409 reduced ABP post IE training interventions. Prior research demonstrated significant 410 improvements in cardiac autonomic regulation (reduced sympathetic activity) and post 411 exercise reductions in ABP, following a single bout of bilateral isometric hand-grip exercise 412 (24). Post exercise hyperaemia and associated sheer stress, mediating increased nitric oxide 413 bioavailability are other potential mechanisms (36). Together these physiological responses 414 reduce peripheral vascular resistance, which reduces cardiac after-load and improves LV 415 haemodynamics.

416

417 Our results contrast the findings of previous research, which utilised the isometric hand grip 418 test to induce an increase in LV after-load and assess LV twist mechanics (41). In this study, 419 isometric hand-grip exercise produced a significant transient increase in ABP and LV end 420 systolic volume. The increased after-load induced significant reductions in LV systolic and 421 diastolic function and significant reductions in apical rotation, basal rotation and LV twist 422 and untwist mechanics. However, the authors recorded echocardiographic data during the 423 isometric contraction, as opposed to the recovery period, which was performed in our study. 424 Similar results were reported with a single isometric hand-grip exercise session followed by a period of post-exercise circulatory occlusion (3). Studies by both Weiner et al. (2012) and 425

Balmain et al. (2016) in healthy populations confirm data from clinical populations, where a
decrease in cardiac mechanics is associated with an increase in LV after-load (35), which is
an important finding when considering the continuum of hypertensive heart disease from
raised after-load to adverse LV remodelling to cardiac failure. It is conceivable that had
Weiner et al. (2012) recorded data in the recovery period they may have produced similar
results to this study, since ABP reduced below baseline in the recovery period.

432

433 Study limitations

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435 Our study is limited by a small sample size and comprised only male, Caucasian participants. 436 We acknowledge that maximal IE tension was not recorded due to the fact that the wall squat 437 does not use external resistance as a means of determining exercise intensity. However, the 438 wall squat method used in this study has been shown to produce similar heart rate responses 439 to other lower limb IE protocols and also produce significant reductions in resting blood 440 pressure. Therefore, it is feasible to suggest that participants produced similar tension to that 441 documented in previous IE research where tension equated to approximately 24% maximal 442 voluntary contraction when using 95% heart rate peak (9). Speckle tracking 443 echocardiography has inherent limitations and the exact location of the basal and apical 444 planes may be different from patient to patient. The acute responses highlighted may simply 445 be a consequence of improved LV contractility and reduced after-load. Nevertheless, the 446 findings are still of significant interest since IE training interventions have been shown to 447 reduce after-load, which may elicit long-term improvements in myocardial performance. 448 However, whether these acute responses translate into sustained cardiac adaptations is as yet 449 unknown.

450

451 Clinical perspective

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453 Arterial hypertension can induce a progressive deterioration in cardiac performance and is the 454 leading modifiable risk factor for premature mortality globally (47). Pre-HTN is highly 455 prevalent and is associated with a higher incidence of cardiovascular disease compared to 456 optimal blood pressure (38). IE training interventions result in greater reductions in ABP 457 compared with traditional exercise modalities (7) and is a short duration exercise intervention 458 that can be performed in the home. This study demonstrates that a single IE training session 459 results in acute improvements in LV remodelling, LV function and mechanics. The long-term 460 adaptation of the LV to IE training interventions remains unknown. However, these acute 461 favourable responses provide an insight into the observed reductions in ABP after a period of 462 IE training. These results may in turn be partly responsible for the observed reductions in 463 ABP following IE training programmes. Although further work is needed, this study supports 464 the potential role for IE training as a valid treatment for blood pressure lowering.

465

466 **Conclusion**

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A single IE training session was associated with significant changes in cardiac remodelling, function and LV mechanics in a population with pre-HTN. The acute cardiac responses seen may be clinically important and help further our understanding of the mechanisms inducing blood pressure reductions and improving cardiovascular health following IE training. Future short and long-term IE training interventions are needed in order to understand the implications of these acute cardiac responses.

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479	
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481	author(s).
482	
483	Author Contributions
484	
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486	performed experiments; J.O'D, K.A.T. and R.S. analysed data; J.O'D, K.A.T, J.D.W.,
487	D.A.C., and R.S. interpreted results of experiments; J.O'D prepared figures; J.O'D, K.A.T
488	and R.S. drafted manuscript; J.O'D, K.A.T, J.D.W., D.A.C., and R.S. edited and revised
489	manuscript; J.O'D, K.A.T, J.D.W., D.A.C., and R.S. approved final version of manuscript.
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673 Figure Legends

Figure 1: Knee joint angles used for the five consecutive 2-minute stages of the incremental
isometric exercise test (left to right: 135°, 125°, 115°, 105°, and 95°).

Figure 2: Representative short axis images and speckle tracking imaging. Strict imaging criteria was utilised in order to standardise all parasternal short axis images. (A) An adequate basal image was defined by the presence of full thickness myocardium surrounding the mitral valve at end systole. (B) The left ventricular (LV) apex was obtained by moving the transducer one to two intercostal spaces caudally from the basal position to align with the apical short axis with no visible papillary muscles that closely approximated an end-diastolic ratio of LV cavity diameter to total LV diameter of 0.5, as described previously (40). The endocardium was traced manually on the 2-dimensional image and the speckle tracking software automatically tracked myocardial motion and only acceptable tracking was accepted as shown in (C) basal and (D) apical short-axis images. Figure 3: Sequential representation of left ventricular twist, basal and apical rotation pre and post isometric exercise training. Annotations indicate key findings and for clarity statistical differences have not been displayed; refer to table 2. Note: AVC, aortic valve closure.

Structural Parameters	Pre-IET	Post-IET	P Value
LV internal diameter diastole (cm)	4.98 ± 0.4	5.09 ± 0.47	0.42
LV internal diameter systole (cm)	3.4 ± 0.2	3.09 ± 0.3	0.002
IVSd (cm)	0.98 ± 0.1	0.93 ± 0.1	0.16
LVPWd (cm)	0.99 ± 0.1	0.9 ± 0.1	0.013
Relative wall thickness	0.4 ± 0.06	0.36 ± 0.05	0.018
LV mass (g)	177.8 ± 31.7	164.6 ± 26.8	0.16
LV mass index $(g \cdot m^2)$	86.3 ± 15	80 ± 13.8	0.18
LV geometry			
Normal	18	24	0.035
Concentric remodelling	8	2	
LV length (cm)	8.9 ± 0.6	8.8 ± 0.7	0.7
Global LV diastolic function			
Peak E velocity (cm·s ⁻¹)	0.7 ± 0.1	0.74 ± 0.2	0.32
Peak A velocity $(cm \cdot s^{-1})$	0.5 ± 0.2	0.51 ± 0.2	0.82
Peak E/A ratio	1.48 ± 0.3	1.53 ± 0.4	0.69
Isovolumic relaxation time (ms)	77.2 ± 15	82.1 ± 23	0.67
Global LV systolic function			
Left ventricular ejection fraction (%)	60.8 ± 3	68.3 ± 4	< 0.001
Fractional shortening (%)	31.6 ± 4.5	39.9 ± 5	< 0.001
Heart rate (b·min ⁻¹)	62 ± 9.4	63 ± 7.5	0.63
Stroke volume (mL)	74.6 ± 11	96.3 ± 13.5	< 0.001
Cardiac output (L⋅min ⁻¹)	4.3 ± 0.7	6.1 ± 1	< 0.001
LV tissue Doppler			
Average peak E' $(m \cdot s^{-1})$	0.12 ± 0.02	0.15 ± 0.03	< 0.001
Average peak A' (m·s ⁻¹)	0.1 ± 0.02	0.11 ± 0.02	0.05
Average peak S' $(m \cdot s^{-1})$	0.09 ± 0.01	0.19 ± 0.04	< 0.001
LV filling pressures			

Table 1: Left ventricular function from standard and tissue Doppler echocardiography

	Average E/E' ratio	6.08 ± 1.87	5.01 ± 0.82	0.006
Art	terial pressures			
	Systolic (mmHg)	132.6 ± 5.6	109.4 ± 19.6	< 0.001
	Diastolic (mmHg)	77.6 ± 9.4	58.8 ± 17.2	< 0.001
	Mean (mmHg)	94.7 ± 10.1	78.8 ± 18	< 0.001
698 699	Note: LV = Left ventricular; IVSd = Interv posterior wall thickness diastole.	ventricular septal thickness diastole	; LVPWd = Left ventr	icular
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	Pre-IET	Post-IET	P Value
LV longitudinal parameters			
Peak global LV longitudinal strain (%)	-17.8 ± 2.4	-20 ± 1.8	0.002
Peak global LV longitudinal strain rate (%·s ⁻¹)	$\textbf{-0.88} \pm 0.1$	-1.03 ± 0.1	< 0.001
Peak global LV longitudinal strain rate diastole ($\% \cdot s^{-1}$)	1.26 ± 0.3	1.37 ± 0.3	0.259
LV basal parameters			
Basal rotation (°)	-5 ± 3.5	-7.22 ± 3.3	0.047
Basal systolic rotational velocity (°·s ⁻¹)	-51 ± 21.9	-79.3 ± 41.3	0.01
Basal diastolic rotational velocity (°·s ⁻¹)	48.7 ± 18.9	62.3 ± 21.4	0.042
Basal radial strain (%)	48.6 ± 22.9	55.5 ± 19.4	0.305
Basal radial strain rate $(\% \cdot s^{-1})$	3.3 ± 1.2	3.9 ± 1.8	0.205
Basal circumferential strain (%)	-28.9 ± 5.4	-34.8 ± 6.3	0.003
Basal circumferential strain rate $(\% \cdot s^{-1})$	-2.3 ± 0.5	-2.8 ± 0.6	0.009
LV apical parameters			
Apical rotation (°)	6.58 ± 4.5	7.8 ± 4.4	0.389
Apical systolic rotational velocity (°·s ⁻¹)	52.1 ± 22.1	60.5 ± 26	0.278
Apical diastolic rotational velocity (°·s ⁻¹)	-42.2 ± 18.3	-57.9 ± 31.7	0.062
Apical radial strain (%)	35.4 ± 16.4	55 ± 17.8	0.001
Apical radial strain rate $(\% \cdot s^{-1})$	3 ± 1.6	3.6 ± 1.5	0.17
Apical circumferential strain (%)	-25.3 ± 4.1	-32.9 ± 7.6	< 0.001
Apical circumferential strain rate $(\% \cdot s^{-1})$	-2.04 ± 0.5	-2.57 ± 0.7	0.012
LV twist parameters			
Twist (°)	10.4 ± 5.8	13.8 ± 5	0.049
Systolic twist velocity (°·s ⁻¹)	69.6 ± 27.5	98.8 ± 35.8	0.006
Untwist velocity (°·s ⁻¹)	-64.2 ± 23	-92.8 ± 38	0.007
Torsion (°· cm ⁻¹)	1.46 ± 0.86	2.07 ± 0.88	0.032
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Table 2: Myocardial mechanics pre and post isometric exercise training

720 Note: LV = Left ventricular.